

1 **Facile synthesis of MoS₂ nanoflower-Ag NPs grown on lignin-**
2 **derived graphene for Troponin I aptasensing**
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4 **Mugashini Vasudevan^{1,2}, Sathaniswarman Remesh^{1,2}, Veeradasan Perumal^{1,2,*},**
5 **Pandian Bothi Raja³, Mohammad Nasir Mohammad Ibrahim³, Subash C.B.**
6 **Gopinath^{4,5}, Saravanan Karuppanan² and Mark Ovinis⁶**

7
8 *¹Centre of Innovative Nanostructures and Nanodevices (COINN), Universiti*
9 *Teknologi PETRONAS, 32610 Seri Iskandar, Perak Darul Ridzuan, Malaysia*
10

11 *²Department of Mechanical Engineering, Universiti Teknologi PETRONAS, 32610*
12 *Seri Iskandar, Perak Darul Ridzuan, Malaysia*
13

14 *³School of Chemical Sciences, Universiti Sains Malaysia, 11800, Penang, Malaysia*
15

16 *⁴Institute of Nano Electronic Engineering, Kangar 01000 & Faculty of Chemical*
17 *Engineering & Technology, Arau 02600, Universiti Malaysia Perlis (UniMAP), Perlis,*
18 *Malaysia*
19

20 *⁵Micro System Technology, Centre of Excellence (CoE), Universiti Malaysia Perlis*
21 *(UniMAP), 02600 Arau, Pauh Campus, Perlis, Malaysia.*
22

23 *⁶School of Engineering and the Built Environment, Faculty of Computing,*
24 *Engineering and the Built Environment, Birmingham City University, B4 7XG, UK*
25

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27
28
29
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32 **Corresponding email: veeradasan.perumal@utp.edu.my (Ph: +6010-3773747)*
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34 **ABSTRACT**

35 This article presents the development and application of a green lignin-derived graphene
36 biosensor for Troponin I, a biomarker for Acute Myocardial Infarction (AMI). The graphene was
37 synthesized from oil palm lignin through an optimized laser scribing process. While the three-
38 dimensional nature of the laser-scribed lignin-derived graphene (3D LSG) is advantageous, it
39 suffers from poor electrical conductivity due to the amorphous nature of lignin. Therefore,
40 semi-conductive molybdenum disulphide (MoS_2) precursor with conductive green silver
41 nanoparticles (Ag NPs) was added to 0.5, 1.0, 1.5, and 2.0 grams of 3D LSG to synthesize
42 3D LSG_MoS₂_Ag NPs hybrids via an aqueous hydrothermal process. Morphological,
43 physical, and structural analyses showed the presence of petal-like MoS_2 nanoflower with Ag
44 NPs on the 3D LSG surface. The strong interrelation between 3D LSG, MoS_2 , and Ag NPs
45 was confirmed by X-ray spectroscopy, Raman spectroscopy and energy dispersive
46 spectroscopy (EDS). Specifically, X-ray spectroscopy revealed the formation of O1s, Ag 3d,
47 C1s, Mo 3d, and S2p in the 3D LSG_MoS₂_Ag NPs-2.0 hybrid. Raman spectroscopy revealed
48 an enhancement in the surface area of the 3D LSG_MoS₂_Ag NPs-2.0 hybrid, which
49 enhances the detection sensitivity. The 3D LSG_MoS₂_Ag NPs hybrid was subsequently
50 chemically modified and immobilised with an aptamer to interact with Troponin I on an
51 impedimetric sensor. The 3D LSG_MoS₂_Ag NPs hybrid showed high analytical performance,
52 high specificity, and a ~4-fold increment in selectivity, with a detection limit of 100 attomolar.
53 This biosensor has a sensitivity of $31.45 \mu\text{A mM}^{-1} \text{cm}^{-2}$, stability of 87%, with a relative standard
54 deviation for reproducibility of 3.8%.

55 **Keywords:** *Laser scribed graphene; Biopolymer; Nanosensor; Electrochemistry; Biomarker;*
56 *Acute Myocardial Infarction*

57 **1.0 Introduction**

58 According to the World Health Organisation (WHO), acute myocardial infarction (AMI) has one
59 of the highest mortality rates, responsible for almost 17.9 million deaths every year [1]. Early
60 treatment of AMI significantly improves prognosis, as it prevents additional damage to the
61 heart. AMI is detected by evaluating the concentration of AMI biomarker (Troponin I) in the
62 human blood system. As such, a quick, cost-effective, and precise AMI biosensor is needed
63 to detect the AMI biomarker in patients experiencing AMI symptoms. The alternative is having
64 to wait in line for the traditional clinical method such as electrocardiography (ECG), angiogram
65 and blood test. In that regard, the development of an readily accesible biosensor to detect AMI
66 is a promising approach to overcoming the high mortality rates [2]. Three main factors need
67 to be considered to create a biosensor: the active material/substrate, transducer/bioelectrode,

68 and bioreceptor-target interactions [3]. Optimizing the active material/substrate is the most
69 challenging factor and is an active research area. The nanomaterials mainly used in AMI
70 biosensors are conducting polymer [4], gold nanoparticles [5], boron nitride quantum dots [6]
71 and zinc oxide [7]. Utilizing these nanomaterials improves the analytical performance of an
72 AMI biosensor. However, these nanomaterials are chemical-based, expensive, difficult to work
73 with, and not green.

74 The discovery of graphene by Geim and Novoselov has opened the doors of opportunities to
75 create carbon-based biosensor nanomaterials [8–11]. Graphene is used for biological and
76 chemical sensing due to its excellent electrical conductivity, physiochemical properties, and
77 morphological structure [12]. The commonly used methods to synthesize graphene are
78 chemical vapour deposition (CVD), and mechanical and chemical exfoliation. However, these
79 methods need high temperatures, high energy, highly volatile precursors, increased usage of
80 toxic chemicals, and are time-consuming [13,14]. Therefore, an alternative, simple,
81 straightforward method, like laser scribing, was introduced to synthesize graphene. The laser
82 scribing (LS) method is a direct one-step conversion method to produce graphene from
83 polyamide films through pulsed ultraviolet laser scribing treatment [15]. The LS method rapidly
84 produces graphene on a large scale in a short time with excellent productivity and
85 reproducibility [16]. However, the fabrication of graphene from polyamide using the LS method
86 has limitations in terms of harmfulness to the environment, requiring large resources, and
87 forms large polyamide waste after the service lifetime.

88 Biomass is an ideal material to replace polyamide as an LS substrate, as lignin is an abundant
89 renewable resource, cost-effective, biodegradable, and environmentally friendly [17]. In lignin-
90 derived graphene through the LS method, biowaste lignin is converted into graphene under a
91 visible CO₂ laser [18]. Lignin biomass has remarkable characteristics such as high thermal
92 stability, high carbon content, biodegradability, excellent physical /chemical properties, and
93 good stiffness. It is a natural reducing agent, making it an attractive green polymer material
94 for biosensing applications [19]. Recent breakthroughs have enabled the development of
95 microporous three-dimensional (3D) graphene from lignin biopolymer through the LS method.
96 The unique interconnected sandwich network structure of 3D graphene from lignin possesses
97 a large surface area, and high mechanical strength and is compatible with other materials.
98 Even so, lignin-derived graphene does not have commercial-grade graphene electrical
99 conductivity, due to the amorphous nature of lignin [20].

100 Silver nanoparticles (Ag NPs) are extensively used nanoparticles in biosensor applications
101 due to their unique physical and chemical properties. Ag NPs have attracted significant
102 attention as nanocomposites for surface modification of sensor electrodes. Ag NPs are

103 inexpensive, easy to obtain, have high conductivity, large surface area, high stability, and
104 excellent biocompatibility [21]. In particular, the coupling of graphene with Ag NPs enhances
105 the sensitivity of a biosensor. Furthermore, the adsorption of nanoparticles in graphene
106 prevents the aggregation of graphene sheets [22]. The deposition of Ag NPs on graphene
107 oxide will enhance the electrocatalytic performance and stability of biomolecules. It also
108 overcomes the instability of Ag NPs and the electrical conductivity loss of graphene oxide
109 [23,24]. In that regard, many biosensors were developed using graphene/silver nanoparticles
110 as active material, such as glucose biosensors [25], sulfite biosensors [26], hydrogen peroxide
111 biosensors [27], 4-nitrophenol biosensors [28], adenine and guanine biosensor [29]. However,
112 the use of harmful chemicals and the high-energy consumption needed to synthesize Ag NPs
113 limit their large-scale production.

114 Moreover, highly concentrated reductants and stabilizing agents are needed to reduce the Ag
115 ions into Ag atoms, which then agglomerate into oligomeric clusters leading to the formation
116 of colloidal Ag NPs [30]. The stabilizing agent play a crucial role in the formation of
117 nanoparticles with controlled size and shape. Therefore, a green Ag NPs based biopolymer
118 was introduced in biosensors due to the biocompatible, biodegradable, non-toxic, safe
119 reagents, and decrease in the cost of energy. In a study, Prasad et al. synthesized Ag NPs
120 from the fruits of *Phyllanthus acidus* decorated on reduced graphene oxide (Ag-rGO) to detect
121 dopamine and uric acid [31]. Graphene oxide coupled with pear extract-based green-
122 synthesised silver nanoparticles (Ag-NPs) have been used for the detection of tuberculosis
123 (TB) treatment drugs, ethambutol (EMB) and pyrazinamide (PZA)[32].

124 In this work, transition metal and noble nanoparticles were added to oil palm biowaste lignin-
125 derived graphene, creating a heterostructure hybrid with improved electrical conductivity,
126 chemical reaction, mechanical stability, and electrocatalytic properties. A synergistic
127 combination of molybdenum disulphide (MoS_2) and silver nanoparticles (Ag NPs) was
128 fabricated on lignin-based 3D graphene creating a biosensor with a large surface area and
129 enhanced electron transfer efficiency. / MoS_2 and 3D graphene formed a compact geometric
130 structure owing to their similar sandwich structure with enhanced optical, electrical, and
131 magnetic properties. The intrinsic, large surface area and conductive properties of Ag NPs
132 and MoS_2 improve the immobilisation of biomolecules. Furthermore, the 3D morphology of
133 lignin-based graphene is an advantage for MoS_2 NF to grow vertically, providing more space
134 for Ag NPs bonding and simultaneously improving the graphene's physiochemical properties,
135 which improves the analytical performance of synergistic hybrid in detecting Troponin I. The
136 fabricated hybrid overcomes the severe stacking issues in MoS_2 NF with lignin-based 3D
137 graphene in its precursor.

138 Ag NPs are a promising biocompatible metal for biomarker sensing as they generally
139 conjugate with organic/inorganic materials that protect Ag NPs against agglomeration and
140 improve their electrocatalytic activity and stability, leading to improved electrochemical activity
141 and detection sensitivity [33]. Strong van der Waals force between Ag NPs causes severe
142 aggregation and instability. To overcome the drawbacks of these materials, we developed a
143 heterostructure hybrid of lignin-derived 3D LSG_MoS₂_Ag NPs, via a hydrothermal method
144 to grow MoS₂ nanoflower_Ag NPs on lignin-derived 3D graphene. The morphological, optical,
145 physical, and analytical performance of lignin-derived 3D LSG_MoS₂_Ag NPs for Troponin I
146 biomarkers in human serum were investigated. This research provides new insights into
147 understanding the electrical conductivity and probe-target interaction on advanced biopolymer
148 graphene fabricated hybrid and advances the state of the art in Troponin I biosensing.

149 **2.0 Materials & Methods**

150 *2.1 Materials*

151 Lignin extracted from oil palm's empty fruit bunch was purified [34] for conversion to graphene.
152 Chemicals such as 16-Mercaptohexadecanoic acid, 1-Ethyl-3-(3-dimethylaminopropyl)
153 carbodiimide (EDC), Silver Nitrate (AgNO₃), N-hydroxysuccinimide (NHS), Streptavidin,
154 Phosphate Buffered Saline (PBS), and (3-Aminopropyl) triethoxysilane (APTES) were
155 obtained from Sigma-Aldrich Co., Ltd. (USA). Ammonium Heptamolybdate Tetrahydrate,
156 Thiourea, Potassium Hydroxide (KOH), Ethanolamine, and Ethanol Absolute were obtained
157 from Merck & Co (USA). All these chemicals were used as received without additional
158 purification. The Screen-Printed Carbon Electrode (SPCE) was purchased from Metrohm
159 (Malaysia) Sdn. Bhd. The oligonucleotides were purchased from Avantis Laboratory (USA). A
160 detailed description of the oligonucleotide sequence dilution and characterizations can be
161 found in the supplementary information. The oligonucleotide sequences utilized in this current
162 work are as follows:

163 Probe (Aptamer) – 5' – CGT GCA GTA CGC CAA CCT TTC TCA TGC GCT GCC CCT CTT
164 AAA AAA AAA AAA AAA AAA AAA AAA A-3'; Biotin oligo linker – 5' - / 5Biosg // iC6Sp / TTT
165 TTT TTT TTT TTT TTT TT -3'; Target – Troponin I; Control – Troponin T; Human Serum of
166 male AB plasma were purchased from Sigma-Aldrich Co., Ltd. (USA).

167 *2.2 Synthesis of lignin-based laser-scribed graphene (3D LSG)*

168 Lignin-derived graphene was produced via the laser scribing method [35]. Initially, 20% of the
169 lignin solution was prepared by adding 10 grams of lignin powder in 50 millilitres of distilled
170 water and stirred until a homogenous lignin solution formed. The homogenous lignin solution

171 was coated on a glass substrate and left to dry for 30 minutes in an oven at 50 °C. The dried
172 lignin glass substrate was then inserted in a laser-scribed machine under optimized
173 parameters of 70% laser power, 50% laser speed, and 500% pulse per inch. A CO₂ laser was
174 used to penetrate a lignin-coated glass substrate forming graphene after 30 minutes and the
175 graphene was placed in a desiccator to avoid contamination.

176 2.3 *Synthesis of oil palm lignin-mediated silver nanoparticles (Ag NPs)*

177 Biogenic Ag NPs were synthesised following the experimental procedure reported by M.J.Y.
178 Tai et al.[34]. In brief, a 1000 ppm silver nitrate (Ag NO₃) solution was added gradually to 1000
179 ppm of lignin solution under constant stirring conditions until the homogenous solution
180 changed from dark brown to brownish black, which confirms the reduction of the silver ions to
181 Ag NPs, aided by the lignin. The surface plasmon excitation of Ag NPs causes the colour
182 changes of the solution. This show that the lignin extract could reduce aqueous silver ions to
183 yield stable Ag NPs in water.

184 2.4 *Synthesis of 3D LSG_MoS₂_Ag NPs through a hydrothermal method*

185 The 3D LSG_MoS₂_Ag NPs were prepared accordingly to the previously reported method
186 with a slight modification [36,37]. In brief, 0.6 grams of ammonium heptamolybdate
187 tetrahydrate and 1.77 grams of thiourea were dissolved in 60 ml of distilled water in a beaker.
188 Next, 30 ml of Ag NPs solution and 0.5 gram of 3D LSG were mixed in the same beaker. The
189 resulting mixture solution was stirred for an hour until all the solutes were fully dissolved. Then,
190 the mixture was transferred into a 250 ml Teflon-lined stainless-steel autoclave and heated at
191 a temperature of 200 °C for 24 hours. After the hydrothermal process, the autoclave was left
192 to cool for a few hours. The resultant product, black-coloured 3D LSG_MoS₂_Ag NPs hybrid,
193 was collected thrice, in sequence, through centrifugation using distilled water and ethanol
194 absolute. The 3D LSG_MoS₂_Ag NPs hybrid precipitate was then dried in an oven at 60 °C
195 for 12 hours. A similar procedure was repeated by replacing 0.5 gram of graphene with 1.0
196 gram, 1.5 gram and 2.0 gram of 3D LSG separately. The 3D LSG_MoS₂_Ag NPs hybrid
197 sample was classified as 3D LSG_MoS₂_Ag NPs-0.5, 3D LSG_MoS₂_Ag NPs-1.0, 3D
198 LSG_MoS₂_Ag NPs-1.5 and 3D LSG_MoS₂_Ag NPs-2.0, according to the amount of 3D LSG
199 added. Bare MoS₂ was fabricated using the same procedure without Ag NPs and 3D LSG.

200 2.5 *Immobilisation of biotinylated aptamer on modified SPCE*

201 Chemical modification on SPCE was conducted for aptasensor fabrication. Initially, 10 µL of
202 potassium hydroxide (1 M, pH 9.2) was dropped on SPCE carbon surface and incubated for
203 5 minutes. Next, SPCE/KOH surface was incubated with 10 µL of 2% APTES for an hour to

204 activate the amine surface, followed by incubation with 10 μL of 3D LSG_MoS₂_Ag NPs hybrid
205 for 30 minutes to form a strong covalent bond between amine and the hybrid. 1 mg in 1 ml
206 proportion was then used to dilute functionalized 3D LSG_MoS₂_Ag NPs nanostructure. Next,
207 10 μL of a complex mixture (16-mercaptohexadecanoic acid, NHS, and EDC) was dropped
208 and incubated for an hour to form a stable side reaction with a free functional group for
209 detection of proteins, followed by 10 μL of streptavidin with 30 minutes incubation time. To
210 cap the non-specific interaction sites, 10 μL of ethanolamine was dropped and incubated for
211 30 minutes. Finally, 10 μL of biotinylated aptamer was dropped and incubated for 15 minutes.
212 Biotinylated aptamer was prepared by diluting 2.5 μL of aptamer and biotinylated oligo linker
213 in separate 47.5 μL of pure water. After that, the mixture was combined to form 1 μM of
214 biotinylated aptamer, which was annealed at 60 °C for 1 minute and cooled down at room
215 temperature. The additional oligos in the linker act as a spacer. A buffer solution of 10 mM
216 PBS at pH 7.4 was used to wash after each modification thoroughly. Impedance analysis was
217 conducted to determine the chemical reaction of the assembled molecules on the surface-
218 modified electrode [2,38]. The chemical modification is illustrated in Fig. 1.

219 2.6 *Troponin I hybridization on biotinylated aptamer*

220 The biotinylated aptamer-modified SPCE is now ready to interact with the Troponin I.
221 Concentrations of Troponin I ranging from 100 pM to 100 aM were diluted through serial
222 dilutions. 10 μL of all diluted Troponin I concentrations were dropped one at a time. Each
223 concentration was incubated for 10 minutes and washed thoroughly with 10 mM PBS of pH
224 7.4 to remove the unbonded target. After washing, an impedance analysis was performed.
225 The complete hybridized aptasensor was stored at 4 °C when not in use.

226 2.7 *Determination of Troponin I in protein in Human Serum*

227 A dilution factor of 1:10 000 was used to dilute the Troponin I solution by using the same serial
228 dilution at concentrations ranging from 100 pM to 100 aM to form a Troponin I spiked sample,
229 similar to section 2.5. The rest of the surface modifications and detection strategies employed
230 were identical to the previous section.

231 2.8 *Stability and Repeatability analyses*

232 The stability of the hybridized electrode was determined every week by dropping 10 μL of
233 buffer solution on the surface of the electrode. The repeatability of the electrode was examined
234 by taking measurements using different electrodes from the same batch of preparation for
235 results comparison of every electrode when the aptamer was immobilised on SPCE.

236 **3.0 Results and discussion**

237 Nanoscale 3D LSG was produced from oil palm lignin biopolymer through the laser scribing
238 method with the CO₂ laser penetrating three layers of 20% oil palm lignin solution coated on
239 a glass substrate at optimised parameters. To improve the properties in 3D LSG, MoS₂ and
240 Ag NPs were combined through the hydrothermal method to form a hybrid. Multiple studies
241 were conducted to investigate the growth of MoS₂ vertically on 3D LSG in the presence of Ag
242 NPs. MoS₂ grew on 3D LSG due to its hydrophilic nature. The -OH on the surface of 3D LSG
243 makes for a negative surface charge, which effectively binds with the positively charged Mo
244 precursors by electrostatic interaction [39,40]. Furthermore, the 3D LSG produced through the
245 laser scribing process exhibits a unique irregularly spaced structure with porous surfaces that
246 enables MoS₂ to attach to the 3D LSG. A reducing agent was not needed because lignin has
247 natural stabilizing and reducing properties [41]. Loading of Ag NPs on 3D LSG can effectively
248 prevent agglomeration, and improved the dispersion/stability of the materials in
249 physiochemical solutions. The formation of numerous soft Lewis base sites in the form of
250 sulphur atoms in MoS₂ leads to a strong attraction to Ag⁺ ions, easily forming Ag-S bonds
251 [42].

252 Lignin is composed of numerous functional groups, such as reductive aliphatic hydroxyls and
253 phenolic hydroxyls. Each of these can potentially reduce or cap silver nanoparticle synthesis.
254 Also, these functional groups serve as binding sites for Ag⁺ ions and act as a natural reducing
255 agent. The phenolic hydroxyl group has high potential to reduce silver cations into silver
256 nanospheres while the sulfonate groups of lignin induce the dispersion of the formed
257 nanoparticles in an aqueous solution. Thus, the lignin stabilizes the nanoparticles and
258 prevents agglomeration due to its three-dimensional network structure [43,44]. Furthermore,
259 traditional methods used a reducing agent such as hydrogen peroxide and sodium
260 borohydride to synthesize silver nanoparticles. These chemicals are toxic to the environment
261 if not disposed of in a proper manner. We utilized a green silver nanoparticle by deriving from
262 lignin biopolymer without using a reducing agent, as lignin has natural reducing properties.
263 The lignin-derived silver nanoparticles have a uniformed spherical shape and no
264 agglomeration, as shown in Fig. S2 (e-f). Also, it is biocompatible, biodegradable and friendly
265 to the environment. The MoS₂_Ag NPs-decorated on 3D LSG offers unrivalled nanostructures
266 that can heighten the separation efficiency of the electron-hole pairs having higher catalytic
267 activity, sensitivity, and stability for Troponin I aptasensing.

268 *3.1 Field-Emission Scanning Electron Microscopy (FESEM)*

269 FESEM was used to study the general morphology of the as-synthesized MoS₂_Ag NPs-
270 decorated on a 3D LSG hybrid. The 3D LSG_MoS₂_Ag NPs hybrid, synthesized by a

271 hydrothermal method at different doping amounts of 3D LSG, were classified as 3D
272 LSG_MoS₂_Ag NPs-0.5, 3D LSG_MoS₂_Ag NPs-1.0, 3D LSG_MoS₂_Ag NPs-1.5, and 3D
273 LSG_MoS₂_Ag NPs-2.0 respectively corresponding to the doping amounts of 3D LSG. The
274 result in Fig. 2(a-b) shows the MoS₂ nanoflower is dominant with high density in 3D
275 LSG_MoS₂_Ag NPs-0.5. The shape and size of MoS₂ nanoflower vary, with a diameter range
276 of 0.5 to 2.5 μm. However, in Fig. 2c, clumps MoS₂ surrounding the 3D LSG surface were
277 found. The growth of MoS₂ nanoflower vertically on the surface of 3D LSG is attributed to the
278 high surface roughness shown in Fig. 2d [45]. More clumps with bigger diameters can be seen
279 in Fig. 2(e & g), as the doping amount of 3D LSG increases. 3D LSG with mesopores has a
280 large surface area which can boost the electrochemical performance and attracts MoS₂ to
281 grow on its surface [46]. The close-up view in Fig 2 (f & h) reveals the incorporation of smaller
282 MoS₂ nanoflower with a diameter range of 0.2 to 2.5 μm on the irregular shape of 3D LSG,
283 forming an interconnected conductive network which ensures optimum convection during the
284 heating process. A well-stacked MoS₂ nanoflower on 3D LSG was observed due to van der
285 Waals interaction which overcomes the severe stacking issues of MoS₂ [47,48]. The TEM
286 results are provided in the supplementary information (Fig. S1). The variation in the MoS₂ size
287 is due to the number of nanopetals curved around it. MoS₂ is an interlayered nanomaterial
288 that grew as a layer-by-layer pattern along the preferred curly growth direction during the
289 hydrothermal process, forming several single MoS₂ nanoflowers, with growth continuing until
290 a critical thickness was reached, which then causes aggregation of MoS₂ to occur. During the
291 growth of smaller nanoflowers or petal shape grains, they absorb thermal energy and start
292 coalescing or fusing to form bigger grains. The bigger and fluffy grains provide more void
293 space and numerous active sites, which could buffer the volume changes during the
294 intercalation-deintercalation process with added material. The smaller nanoflower provide
295 short pathways and high kinetics for surface modification and aptamer immobilisation. The
296 various size of nanoflower is also accompanied with the changes to their crystallinity, defects,
297 thickness and surface area, which determines the specific capacity. Furthermore, sulfur
298 deficiency could happen during hydrothermal treatment, which destabilize MoS₂, altering the
299 geometry from trigonal prismatic of 2H phase into octahedral of IT phase of MoS₂
300 nanoflowers. The fluffiness of nanoflower was formed due to the lower stacking of nanosheets
301 [49–51]. An observation of lignin nanoparticles on the surface of 3D LSG_MoS₂ with an
302 enhanced magnification of FESEM (Fig.2 (f & h)) reveals that the lignin was not fully converted
303 into graphene during the laser scribing process, leaving some lignin residues. However, these
304 lignin residues are beneficial as a natural reducing and stabilizing agent, which improves the
305 catalytic reaction. The 3D LSG_MoS₂_Ag NPs hybrid provides an efficient path for the
306 chemisorption of biotinylated probe aptamer during immobilization and target (Troponin I)

307 interaction. The FESEM images of 3D LSG, MoS₂, Ag NPs and EDS spectrum of the 3D
308 LSG_MoS₂_Ag NPs hybrids are shown in the supplementary information (Fig. S2 & S3).

309 3.2 X-ray diffraction (XRD)

310 X-ray diffraction (XRD) was conducted to examine the purity, crystallinity, and plane
311 orientation of synthesized 3D LSG, Ag NPs, MoS₂, and 3D LSG_MoS₂_Ag NPs hybrids at
312 different 3D LSG doping amounts. As shown in Fig 3a, the 3D LSG diffraction peaks at broad
313 23.4° (0 0 2), 34.2° (1 0 0), and 45.6° (2 0 0) corresponding to the diffraction peaks of reduced
314 graphene oxide. There is no obvious peak at (0 0 1), indicating a large amount of oxygen-
315 content was removed during the laser scribing process [52,53]. In the XRD pattern of Ag NPs
316 in Fig 3b, the lignin-based Ag NPs have high-intensity peaks at 32.3° (1 2 2) and 35.6° (1 1
317 1), indicating no defects and high crystallinity, compared to short peaks at 67.5° (2 2 0) and
318 75.7° (3 1 1). These peaks refer to crystal planes of Ag, which is in good agreement with face-
319 centered cubic metallic Ag (JCPDS04-0783). Meanwhile, the peaks diffraction in Fig 3c
320 indexed to MoS₂ reveal that MoS₂ is a well-defined hexagonal structure (JCPDS 37-1492),
321 with diffraction peaks at 14.0° (0 0 2), 33.5° (1 0 0), 40.1° (1 0 3), 49.4° (1 0 5) and 58.9° (1 1
322 0). This observation show that MoS₂ are stacked, confirming the layered structure of MoS₂.
323 The broadening of (1 0 3) and (1 0 5) is due to the formation of defects in the nanosized flower.
324 In the pattern of 3D LSG_MoS₂_Ag NPs hybrids, the diffraction peaks of MoS₂ were found in
325 Fig. 3 (d & e) at 13.6° (0 0 2), 33.4° (1 0 0), 39.9° (1 0 3), 49.2° (1 0 5) and 58.5° (1 1 0),
326 whereas in Fig. 3 (f & g) only diffraction planes of (1 0 0) and (1 1 0) with broader peaks were
327 observed, which suggest that MoS₂ dominates the hybrids. However, the diffraction peaks of
328 3D LSG_MoS₂_Ag NPs hybrids were shifted slightly to the left compared to the peaks for
329 MoS₂, indicating the successful blending of 3D LSG and MoS₂. The absence of 3D LSG and
330 Ag NPs diffraction peaks in 3D LSG_MoS₂_Ag NPs hybrids suggests that the doped silver
331 nanoparticles changed the original stacked structure of the 3D LSG and prevented stacking
332 and re-stacking. The intercalations of MoS₂ and Ag NPs on 3D LSG were observed through
333 TEM analysis [37,52,54–56].

334 3.3 Fourier-transform infrared spectroscopy (FT-IR)

335 FT-IR analysis was conducted to determine the functional groups of the prepared materials.
336 Fig. 3 (h-n) depicts the FT-IR spectra of 3D LSG (Fig. 3h), Ag NPs (Fig. 3i), MoS₂ (Fig. 3j) and
337 3D LSG_MoS₂_Ag NPs hybrids at 3D LSG with 0.5 g (Fig. 3k), 1.0 g (Fig. 3l), 1.5 g (Fig. 3m)
338 and 2.0 g (Fig. 3n) of doping. The absorption peaks of 3D LSG_MoS₂_Ag NPs hybrids at
339 different doping amounts of 3D LSG are distinct at 3435.5, 1718.2, 1628.3, 1125.6, 652.5 cm⁻¹,
340 which are assigned to O-H, C=O, C=C, C-O, and Mo-S groups, respectively. Peaks at 667.4,

341 and 758.2 cm^{-1} refer to asymmetric vibration of Mo-O, and the existence of stretching vibration
342 of S-S bond suggests that MoS₂ was successfully loaded. A small peak between 500 – 600
343 cm^{-1} was observed and that attributed to the vibration of Ag-S peak [57]. The hidden short
344 peak of Ag-S bond is due to very little Ag NP added in the MoS₂ precursor. A peak at 1718.2
345 cm^{-1} (C=O bond) in 3D LSG_MoS₂_Ag NPs hybrids confirms the presence of Ag NPs in the
346 hybrids. The broad O-H bond (hydroxyl) at 3435.5 cm^{-1} is similar for all fabricated materials
347 and is caused by the adsorption of water molecules. However, the O-H bond that appeared in
348 3D LSG at 1434 cm^{-1} is absent in 3D LSG_MoS₂_Ag NPs hybrids, indicating a reduction
349 process occurred during the hydrothermal process. The FT-IR analysis of 3D LSG_MoS₂_Ag
350 NPs hybrids has validated the successful pairing of 3D LSG, MoS₂ and Ag NPs in the
351 fabricated hybrids [58,59].

352 3.4 X-ray photoelectron spectroscopy (XPS)

353 XPS studies were performed to reveal the elemental composition and chemical present on the
354 outmost layer of hydrothermally grown MoS₂_Ag NPs on 3D LSG surface. As expected, the
355 wide XPS survey scan of the 3D LSG_MoS₂_Ag NPs-2.0 hybrid has photoelectron peaks of
356 carbon (C), oxygen (O), molybdenum (Mo), sulphur (S) and silver (Ag) (Fig. 4a). The presents
357 of Ag 3p peaks and the slight shift of S 2p peaks in XPS indicate the presence of an Ag-S
358 bond [60,61]. The carbon, C1s spectrum (Fig.4b) of 3D LSG_MoS₂_Ag NPs have peaks at
359 284.8 (C=C and sp² carbon), 286.4 (C-O), 287.5 (C=O) and 289.2 eV (O-C=O). These peaks
360 correspond to the presence of graphene and the interactions of carbon atoms with oxygen,
361 forming carbonyl and epoxide functional groups found at the graphene edges. The epoxy
362 functional groups determine the defects and disorder of graphene structure in the basal plane.
363 The oxygen, O1s spectrum shows the phenolic functional groups found in the hybrid structure
364 at a binding energy of 531.5 (C=O), 533.2 (C-O), and 535.4 (C-OH). The enlarged spectra of
365 Mo 3d are in Fig. 4d and can be deconvoluted to binding energy peaks at 229.1, 232.5, and
366 236.1 eV, which are assigned to Mo⁴⁺ 3d_{5/2}, Mo⁴⁺ 3d_{3/2} and Mo⁶⁺ 3d_{3/2}, respectively. The
367 formation of MoS₂ is identified from the presence of Mo⁴⁺, however, the Mo⁶⁺ is from the
368 surface oxidized and the unconverted molybdenum residues in the precursor forming Mo-O
369 group at peaks 233.5, 234.2 and 236.1 eV. The Mo⁴⁺ peaks confirm the formation of 2H-MoS₂
370 (semiconductor), whereas a peak at 230.5 eV refers to 1T-MoS₂ (metallic). S 2s orbital was
371 also observed at 226.4 eV in Fig. 4d. The Ag peak found in the XPS spectrum of 3D
372 LSG_MoS₂_Ag NPs-2.0 hybrid further confirms the successful attachment of Ag. The
373 corresponding Ag 3d spectra observed from 3D LSG_MoS₂_Ag NPs-2.0 hybrid wide scan are
374 enlarged in Fig. 4e. The Ag 3d XPS spectra consist of two peaks of Ag 3d_{5/2} and Ag 3d_{3/2},
375 which correlate the binding energy peaks at 368.5 and 374.5 eV, attributed to zero valence
376 state. The XPS spectra of three characteristics peaks of S 2p at 162 (S 2p_{3/2}), 163.2 (S 2p_{1/2})

377 and 168.5 (S-O) eV in Fig. 4f reveal the presence of sulphur. The S-O bond appeared during
378 the formation of MoS₂ nanoflower. The XPS analysis confirms the existence and interactions
379 in the 3D LSG_MoS₂_Ag NPs-2.0 hybrid. In short, the conversion of lignin through laser
380 scribing, suggests that graphene oxide is formed. To justify the findings, XPS was conducted
381 to analyse the elemental composition, and chemical and electronic state of oxygen and
382 carbon, with similar composition of commercial graphene oxide found in laser-scribed
383 graphene. The XPS analysis of Mo revealed that the Mo present in the synthesized hybrid
384 exhibits two kind of crystalline phases: hexagonal 2H phase and octahedral 1T phase. 1T-
385 MoS₂ displays much greater chemical/physical properties than natural semiconductor 2H-
386 MoS₂. The element composition of molybdenum (Mo), sulphur (S), and silver (Ag) showed
387 that these elements are present in the synthesized hybrid as a supporting material in improving
388 the physiochemistry of laser-scribed graphene. Additionally, Raman Spectroscopy was
389 performed on the 3D LSG and 3D LSG_MoS₂_Ag NPs-2.0, as shown in supplementary
390 Fig.S4. It shows that 3D LSG_MoS₂_Ag NPs-2.0 hybrid has fewer defects, a large surface
391 area, and greater crystallinity. The higher peaks intensity compared to 3D LSG of 3D
392 LSG_MoS₂_Ag NPs-2.0 hybrid with the addition of MoS₂ and Ag NPs suggest an electron and
393 hole recombination state on 3D LSG surface and the enhancement of graphitization degree
394 attributed to the ablation of heat. The peaks for MoS₂ and broad 2D (presence of Ag NPs)
395 were found in Fig. S4b, confirming the formation of 3D LSG_MoS₂_Ag NPs-2.0 hybrid [62–
396 69]. This hybrid is the most appropriate candidate for further investigation of its analytical
397 performances as a biosensor

398 3.5 *Bio-sensing analyses on 3D LSG/MoS₂/Ag NPs/SPCE*

399 Electrochemical Impedance Spectroscopy (EIS) has been employed to study the biosensing
400 performance of surface-modified 3D LSG_MoS₂_Ag NPs on SPCE in terms of their electrical
401 resistance and interfacial properties. Fig. 5a shows the Nyquist plot of the modified surface of
402 3D LSG_MoS₂_Ag NPs on SPCE. The Nyquist plots can be interpreted by using a fitting model
403 from Randles equivalent circuit. The fitting model is composed of bulk electrolyte resistance
404 (R_a) with a parallel combination of constant phase element (CPE), and charge transfer
405 resistance (R_{ct}) related to the diffusion of ions. The interaction between the interfacial layer of
406 the electrode and electrolyte is represented by the diameter of the semicircle to the magnitude
407 of charge transfer resistance [70,71]. The carbon-filled SPCE chip was initially treated with
408 KOH at 1 M of pH 9.2 to activate the surface of the bare SPCE. In Fig. 5a, the lowest frequency
409 region, the semicircle of APTES, in the impedance spectrum represents R_{ct} =22K Ω. Proper
410 functionalized surface modification over an electrode is needed to ensure a strong stacked
411 bonding for aptamer-troponin I interactions.

412 APTES is a silane that supplies amino acids to functionalize oxide surface (-OH groups). The
413 high surface energy of the oxide surface rapidly interacts and forms a covalent bond with
414 silane molecules [72]. The APTES binds with the -OH group, leaving the amine group
415 unreacted [73]. The amine group of APTES attached to the silver ions found in 3D
416 LSG_MoS₂_Ag NPs hybrid, causing R_{ct} to increase to 27K Ω. The fabricated 3D
417 LSG_MoS₂_Ag NPs hybrid attached to the silane layer through covalent interactions without
418 disrupting the silane structure, as shown in Fig. 1. The Ag NPs linked on NH₂ groups of the
419 APTES covalently [74]. The synthesized hybrid acts as a conductive diffusion pathway in
420 accelerating the charge transfer and reveals the synergistic effect between 3D LSG, semi-
421 conductive MoS₂ and noble metal Ag NPs. The intrinsic conductivity properties of 3D
422 LSG_MoS₂_Ag NPs hybrid tend to have a high energy density, which boosts the electron
423 transfer between the hybrid and electrode. However, the resistance of fabricated 3D
424 LSG_MoS₂_Ag NPs-2.0 hybrid was higher than the APTES, as shown in Fig. 5a.

425 The LSG and Ag NPs were synthesized from lignin biopolymer. Lignin is an amorphous nature
426 biopolymer. The residues of lignin in LSG cause the resistance to be high. The high resistance
427 was due to the unavoidable lignin residues present in LSG. The extra peaks found in Fig. S3
428 are due to the lignin impurities or residues found in the fabricated hybrid material. Several
429 optimizations were conducted to produce high-quality graphene, such as optimizing the lignin
430 concentrations, layers of lignin coated on the glass substrate, and the speed and power of the
431 laser machine. Still, these were unable to remove the lignin residues. The lignin residues can
432 be seen in FESEM in Fig 2. With the increased surface modification of the complex mixture,
433 the R_{ct} value increases. These modifications enable the thiol branch (-SH functional group) of
434 16-mercaptohexadecanoic acid to bind with Ag NPs of 3D LSG_MoS₂_Ag NPs. In contrast,
435 the carboxylic group binds with the amine group of streptavidin, causing the R_{ct} value of
436 complex mixture and streptavidin to be 38K Ω and 46K Ω respectively. NHS and EDC in the
437 complex mixture acts as activators to activate and intensify the surface modified electrode
438 [75]. Besides that, it is also used to stabilize the interaction between amine and carboxyl group
439 (streptavidin). The large surface area of Ag NPs induces charge transfer in biochemical
440 interactions.

441 Ethanolamine was added to the electrode, to block the unoccupied area of the complex
442 mixture to prevent bio-fouling, causing an increase in R_{ct} value to 54K Ω. Ethanolamine acts
443 as a blocking agent to block the unreacted functional groups from the electrode surface that
444 would otherwise compete with reacted functional groups [38]. Usage of blocking agent is
445 necessary to stabilize the Aptamer during immobilisation process and to improve the
446 biosensor's selectivity towards their specific targets. The unique four binding sites feature of
447 streptavidin induces the biotinylated aptamer to bind extensively, forming a strong electrostatic

448 streptavidin-aptamer complex [76]. This complex formation was observed when the R_{ct} value
449 reached 67K Ω . The increment in R_{ct} value of aptamer shows that its immobilisation on
450 streptavidin is a success. Further, an increment in the R_{ct} value is observed when the target
451 (Troponin I) interacted electrode, as shown in Fig. 5c. These results suggest successful
452 immobilisation and interaction of Troponin I on the aptamer-modified SPCE electrode. The
453 increment in the EIS is induced by a relatively larger biomolecule complex formation on the
454 electrode surface. Creating suitable surface chemistry to immobilise or capture biomolecules
455 on the 3D LSG_MoS₂_Ag NPs will aid the detection and monitoring of various biomarkers.

456 The resistances and electrical conductivity of the 3D LSG_MoS₂_Ag NPs hybrids were
457 determined through electrochemical impedance spectroscopy (EIS) measurements. Fig. 5b
458 shows the Nyquist plot of four hybrid variations (3D LSG_MoS₂_Ag NPs-0.5, 3D
459 LSG_MoS₂_Ag NPs-1.0, 3D LSG_MoS₂_Ag NPs-1.5 and 3D LSG_MoS₂_Ag NPs-2.0) that
460 differ in 3D LSG doping amounts. The EIS of the surface-modified SPCE electrode was
461 performed at room temperature. The diameter of the semicircle formed for each hybrid
462 corresponds to the charge transfer resistances (R_{ct}) caused by the redox reaction. The
463 intersection of the semicircle at the X-axis indicates the equivalent series resistance (R_s) of
464 the electrode materials. The Nyquist plot in Fig. 5b revealed that 3D LSG_MoS₂_Ag NPs-2.0
465 has the smallest semicircle with the lowest R_{ct} value of 28K Ω , due to ideal capacitive
466 behaviour compared to other 3D LSG_MoS₂_Ag NPs hybrids. The enrichment amount of 3D
467 LSG directly affects the charge transfer and conductivity of 3D LSG_MoS₂_Ag NPs-2.0
468 because the 3D LSG has electrical conductivity, which means electrons transfer happens
469 when it is in use. Still, it is not up to standard commercial-grade graphene. Due to this, the
470 addition of supporting materials like MoS₂ and Ag NPs is required to improve the conductivity
471 of the LSG.

472 Furthermore, the addition of 3D LSG aids in the aggregation-free growth of MoS₂ on 3D LSG,
473 which eventually increases the nucleation sites for MoS₂ growth on 3D LSG and further
474 accelerates the ionic conductivity, as more charge carriers are formed. In addition, 3D LSG
475 has excellent enrichment ability for organic molecules and has an attractive chemical
476 enhancement effect. The large number of MoS₂ edges act as active catalytic sites, which
477 leads to excellent electrical coupling between MoS₂ and the underlying 3D LSG network. The
478 synergistic effect of Ag NPs on MoS₂ opens more interparticle gaps, which creates a
479 conducive surface for the interaction of biomolecules. The addition of less than 2.0 gram of
480 3D LSG (3D LSG_MoS₂_Ag NPs-0.5, 3D LSG_MoS₂_Ag NPs-1.0 and 3D LSG_MoS₂_Ag
481 NPs-1.5), results in the repulsion of electron transfer, and the gradual loss of conductivity. The
482 Nyquist plot highlights the improvement in ion diffusion and charge transfer characteristics
483 within electrodes due to a higher 3D LSG loaded amount. The 3D LSG_MoS₂_Ag NPs-2.0

484 hybrid is therefore the best hybrid material for immobilisation and interaction of probe and bio-
485 target to detect Troponin I.

486 Fig. 5c shows the impedimetric semi-circle response of aptamer-modified 3D LSG_MoS₂_Ag
487 NPs bio-electrode hybridized with concentrations of the complementary target (Troponin I)
488 ranging from 100 attomolar (aM) to 100 picomolar (pM). The value of charge transfer
489 resistance (R_{ct}) increases significantly with increasing concentrations of Troponin I, due to a
490 significant rise in bio-conjugation between aptamer and Troponin I. The resultant R_{ct} confirms
491 the successful detection of a linear range (100 aM to 100 pM) of Troponin I on aptamer-
492 modified bio-electrode, demonstrating the superiority of the sensing elements. The excellent
493 bio-sensing mechanism of 3D LSG_MoS₂_Ag NPs-2.0 is because 3D LSG has a large surface
494 area with MoS₂ nanoflowers on its surface that provides a platform for high catalytic activity.
495 Furthermore, the binding of Ag at the sulphur atom of MoS₂ improves the electrocatalytic
496 capability of the hybrid. The addition of Ag NPs avoids the need for a stabilizer or reducing
497 agent for biomolecular immobilisation on modified bio-electrode. Hence, the coupling of 3D
498 LSG, MoS₂ nanoflower and Ag NPs accelerated the charge transfer properties, which resulted
499 in unparalleled electrochemical performances.

500 Various concentrations of human serum were prepared to evaluate the impedimetric
501 semicircle response of aptamer-modified bio-electrode that was able to hybridize with the
502 specific Troponin I nucleic acid sequence under the same experimental conditions as the
503 target in Fig. 5c. The Nyquist plot, as shown in Fig. 5d, shows a similar charge resistance
504 increment with the increasing concentrations of the target in human serum, upon aptamer-
505 target interaction. The similar semicircle trend with target concentrations revealed that the
506 aptamer-modified 3D LSG_MoS₂_Ag NPs bio-electrode exhibits high specificity for Troponin
507 I detection in human serum, with the presence of an abundance of other biomolecules in the
508 human serum. The performance of the aptamer-modified 3D LSG_MoS₂_Ag NPs biosensor
509 was differentiated and compared with previously reported biosensors for Troponin I detection.
510 The values are given as supplementary information (Table S1) with the aptamer-modified 3D
511 LSG_MoS₂_Ag NPs biosensor more selective compared to other studied biosensors.

512 3.6 Analytical performances of 3D LSG_MoS₂_Ag NPs_SPCE biosensor

513 The sensitivity of the 3D LSG_MoS₂_Ag NPs_SPCE biosensor and linear correlation of
514 differences in the charge transfer resistance, g with the logarithm of Troponin I concentrations
515 (Fig. 6a) was investigated. It was observed that R_{ct} increases linearly with increasing Troponin
516 I concentrations from 100 aM to 100 pM. The R_{ct} at aptamer for immobilized bio-electrode
517 and hybridized bio-electrode were found to be directly proportional to the logarithm of target
518 concentrations, with a linear equation of $y = 3.95286E4 + 3.62927E4x$, ($R^2 = 0.9876$). The

519 linear regression, R^2 shows that the sensor has good linearity with target concentration
520 increment. The sensitivity was calculated using the following equation [77]:

$$\begin{aligned} &521 \\ &522 \text{Slope of calibration plot, } m \text{ (}\mu\text{A } \mu\text{M}^{-1}\text{)} \\ &523 \text{Sensitivity} = \frac{\text{Slope of calibration plot, } m \text{ (}\mu\text{A } \mu\text{M}^{-1}\text{)}}{\text{Active Surface Area, } A \text{ (cm}^2\text{)}} \\ &524 \end{aligned}$$

525
526 with respect to the logarithm of Troponin I concentration, as shown in Fig. 6a. It was observed
527 that the R_{ct} linearly increases as the Troponin I concentrations increase from 100 pM-100 aM
528 and thereafter saturated further. The sensitivity of 3D LSG_MoS₂_Ag NPs_SPCE biosensor
529 is 31.45 $\mu\text{A mM}^{-1} \text{cm}^{-2}$ for a SPCE active surface area of 0.1257cm² [2]. The limit of detection
530 (LOD) of the 3D LSG_MoS₂_Ag NPs biosensor was 100 aM, estimated using a signal-to-noise
531 ratio of more than 3σ (where σ is the standard deviation of the blank solution, $n=5$). The
532 selectivity of 3D LSG_MoS₂_Ag NPs biosensor was evaluated by dropping human serum on
533 aptamer-modified 3D LSG_MoS₂_Ag NPs bio-electrode in the presence of various proteins.
534 Fig. 6b shows that the aptamer-modified 3D LSG_MoS₂_Ag NPs bio-electrode hybridized with
535 Troponin I only, with a rise in R_{ct} values compared to immobilisation of Troponin T and other
536 proteins. The charge transfer resistance displayed a ~4-fold increase in selectivity, as the
537 aptamer only captures Troponin I, although other biomolecules were present.

538 Troponin I level in normal healthy human blood is <0.04 ng/ml and >0.40 ng/ml after an AMI,
539 well within the limit of detection for the current biosensor. The aptamer is designed to capture
540 or interact with the specific Troponin I target. Further, the blocking step prevents the non-
541 specific attachment of biomolecules on the sensing surface. Every material added to the SPCE
542 chip has its own incubation time. After the incubation time, the extra and unbounded material
543 will be washed before taking the impedance reading. Through washing, the interference of the
544 electrode surface will be avoided and could prevent the resistance increment on the electrode
545 surface. Furthermore, selectivity test on the developed biosensor was conducted using human
546 serum, as shown Fig. 6b. The selectivity test demonstrated that the designed aptamer
547 captures only Troponin I in human serum, even when other biomolecules are present. As a
548 result, the developed biosensor has a high selectivity. The 3D LSG_MoS₂_Ag NPs biosensor
549 showed good repeatability with a relative standard deviation (RSD) of 3.8% for five parallel
550 devices prepared under a similar procession procedure, as shown in Fig. 6c. The shelf-life of
551 the electrode was investigated by checking the stability of a hybridized electrode for six weeks
552 stored at a temperature 4 °C. The stability analysis shows that the sensor used in the current
553 work is stable and exhibits stability of 87% after six weeks (Fig. 6d).

554 **4.0 Conclusion**

555 A biopolymer-based hybrid for biosensing has been reported in this study, with large active
556 surface area, high sensitivity, and excellent electrical characteristics. The combination of 3D
557 LSG with MoS₂ and Ag NPs resulted in an exceptional active material/substrate. MoS₂ and Ag
558 NPs were introduced to enhance the poor conductivity of 3D LSG. Morphological observation
559 and structural analyses revealed petal-like MoS₂ with embedded Ag NPs on the 3D LSG
560 surface. Impedimetric analysis revealed that the aptasensor attained an attomolar level of
561 detection with excellent selectivity detection of Troponin I. In addition, 3D LSG_MoS₂_Ag NPs
562 hybrid has remarkable features, which can enhance the immobilisation of aptamer due to its
563 large surface area enabling the capture of more Troponin I biomolecules. Furthermore,
564 biopolymer-based 3D LSG forms a high-affinity alternative material to non-renewable
565 graphene, with the addition of MoS₂ and Ag NPs improving the interaction between the
566 aptamer and Troponin I. This biopolymer-based biosensor will open new pathways in
567 developing green-based biosensors for non-invasive diagnostic systems. Laser scribing is a
568 promising one-step method for producing lignin-derived graphene. However, due to lignin
569 residues in the final product, lignin-derived graphene has slightly higher resistance than high
570 pristine graphene. In our work, we have optimised the process to produce high-quality
571 graphene by optimising lignin concentrations, layers of lignin coated on glass substrate, laser
572 machine speed and power. However, there are still minor lignin residues present when we
573 fabricate at larger scale. As a result, we concluded that the laser scribing technique is still in
574 its early stages of development and that many parameters need to be optimised before high
575 purity graphene can be produced with no lignin residues. A proper method to convert lignin
576 into 100% graphene through laser scribing will be explored in future to obtain residues-free
577 laser scribed graphene.

578

579 **Acknowledgements**

580 The authors acknowledge the Ministry of Higher Education Malaysia for supporting the
581 research with Fundamental Research Grant Scheme (FRGS) (FRGS/1/2020/TKO/UTP/03/7)
582 and Universiti Teknologi PETRONAS (UTP) for the opportunity to carry out the research in
583 Nanotechnology Research Laboratory and Dye Solar Cell Laboratory.

584 **Author Contributions**

585 Fabrication and development of hybrid microstructures were conducted by M.V. Experiments
586 and drafted manuscript were carried out by M.V with the help of S.R, P.B.R, M.N.M.I, S.C.B.G,

587 M.O, and S.K proof-read the manuscript. V.P supervised the work. All authors analyzed the
588 results and contributed to the discussion presented in the manuscript.

589 **Additional Information**

590 The authors declare no competing financial interests

591 **References**

592

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Figure legends

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866 **Figure 1:** Schematic illustration of the steps involved in the synthesis of aptamer-based 3D
867 LSG_MoS₂_Ag NPs hybrid structure on screen printed carbon electrode (SPCE).

868 **Figure 2:** FESEM images of 3D LSG_MoS₂_Ag NPs hybrid structure. (a) Low and (b) high
869 magnifications images of 3D LSG_MoS₂_Ag NPs-0.5; (c) Low and (d) high
870 magnifications of 3D LSG_MoS₂_Ag NPs-1.0; (e) Low and (f) high magnifications
871 of 3D LSG_MoS₂_Ag NPs-1.5 and (g) Low and (h) high magnifications of 3D
872 LSG_MoS₂_Ag NPs-2.0. The scanning electron microscope uses a focused beam
873 of high-energy electrons up to 30 kV.

874 **Figure 3:** XRD image of (a) 3D LSG, (b) Ag NPs, (c) MoS₂ nanoflower, (d) 3D LSG_MoS₂_Ag
875 NPs-0.5; (e) 3D LSG_MoS₂_Ag NPs-1.0; (f) 3D LSG_MoS₂_Ag NPs-1.5 and (g)
876 3D LSG_MoS₂_Ag NPs-2.0. Showing the semi-crystalline peaks of fabricated
877 nanostructures. FT-IR spectra image of fabricated (h) 3D LSG, (i) Ag NPs, (j) MoS₂
878 nanoflower, (k) 3D LSG_MoS₂_Ag NPs-0.5; (l) 3D LSG_MoS₂_Ag NPs-1.0; (m) 3D
879 LSG_MoS₂_Ag NPs-1.5 and (n) 3D LSG_MoS₂_Ag NPs-2.0. Absorption regions
880 are shown from 400 to 3700 cm⁻¹.

881 **Figure 4:** (a) Survey scan of XPS core level spectra taken on 3D LSG_MoS₂_Ag NPs. The
882 binding energy of (b) carbon, C1s; (c) oxygen, O1s; (d) molybdenum, Mo3d; (e)
883 silver, Ag3d and (d) sulphur, S2p electrons.

884 **Figure 5:** (a) Nyquist plot on surface modifications on SPCE electrode. (b) Nyquist plot of 3D
885 LSG_MoS₂_Ag NPs hybrid nanofibers at 0.5, 1.0, 1.5 and 2.0 g on SPCE
886 electrodes. c) Analysis of the limit of detection. Different concentrations of the target
887 (100 aM to 100 pM) through impedance spectroscopy analysis were shown. (d)
888 Impedance spectra measurement. It is to identify the selectivity of the biosensor.
889 Human serum in the presence of other biomolecules was tested.

890 **Figure 6:** (a) Linear regression curve. Different concentrations of the target with a linear
891 equation of ΔR_{ct} ; (b) A bar diagram on the selectivity of the biosensor and its R_{ct}
892 value; (c) Reproducibility of the biosensor using 5 different SPE electrodes (d)
893 Stability of the biosensor. Tested for 6 weeks against R_{ct} is shown.